

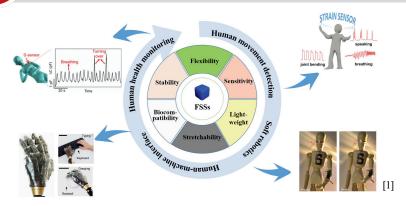
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Bio-based Organohydrogels For Pressure and Strain Sensor Applications

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Objective



This project aims to develop novel bio-based materials that exhibit both stretchability and electrical conductivity, with potential applications in wearable sensing devices for strain and pressure detection. In the initial phase, carrageenan (CG), a bio-derived polymer, was employed as the organohydrogel matrix and integrated with PEDOT:PSS to serve as conductive components within the organohydrogel system.

Methodology

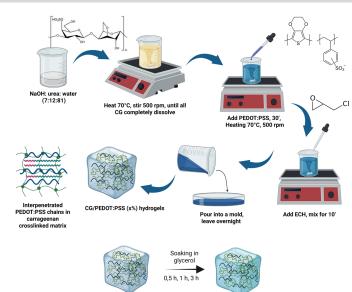


Figure 1. Schematic diagram depicting the preparation of CG_PEDOT:PSS hydrogels, followed by a glycerol immersion treatment to generate CG_PEDOT:PSS organohydrogels.

Results

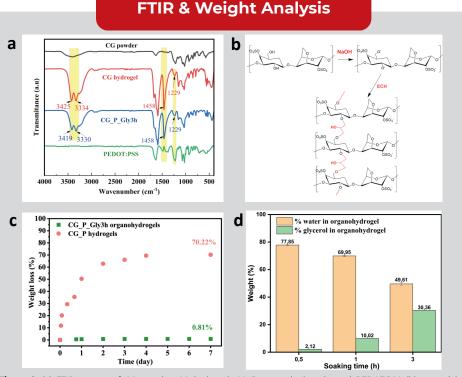


Figure 2. (a) FTIR spectra of CG powder, CG hydrogel, CG_P organohydrogels, and PEDOT:PSS (b) potential mical structure of carrageenan crosslinked by epichlorohydrin; (c) weight loss analysis of CG_P hydrogels and CG_P organohydrogels under a temperature of 21°C and a humidity of 30% for 7 days; and (d) water-to-glycerol weight ratio in organohydrogels with varying soaking times

Electrical and mechanical properties of CG/PEDOT:PSS organohydrogels

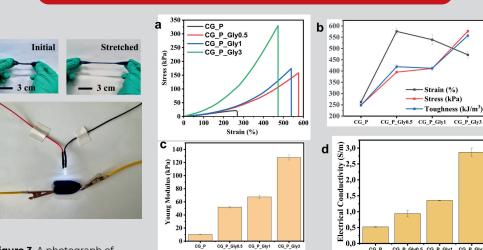


Figure 3. A photograph of CG PEDOT:PSS organohydrogels under stretching and when used as electrical connections to wire a

Figure 4. (a) Stress-strain curves, (b) tensile strain, stress at maximum, and toughness plot, (c) modulus young, and (d) electrical conductivity results of CG_PEDOT:PSS organohydrogels and CG_PEDOT:PSS hydrogels

*CG_P_Gly(x) (Carrageenan_PEDOT:PSS hydrogels soaked x hour in glycerol)

Strain sensing performance CG_P_Gly3h 150 100% 125 AR/R0(%) $r^2 = 0.98759$ 75 $r^2 = 0.99235$ 200 250 100 150 200 250 300 350 Time (s) 0.27 Hz (50% strain Figure 5. Configuration of strain sensor device Figure 6. (a) Change in resistance versus applied strain of CG_PEDOT:PSS_Gly3h; (b) dynamic cyclic test of under varying tensile

strain; (c) relative resistance response to gradually increasing and decreasing strain (d) change in resistance in response to applied strain (50%) with varying strain frequencies.

Pressure sensing performance <7 kPa a y = -2.16x - 0.36 $r^2 = 0.9909$ € -20 7-63 kPa y = -0.58x - 12.27**Organohydrogel** $r^2 = 0.99206$ **Cu-Ni fabric** >63 kPa v = -0.02x - 47.06 $r^2 = 0.99478$ Copper wire 200 150 C Pressure (kPa) d **AR/R0** (%) 1000 500 Time (s)

Figure 7. (a) Configuration of the pressure sensor device; (b) Change in resistance versus applied pressure of CG_P_Gly3; (c) Dynamic cyclic test of CG_P_Gly3h under varying pressures; (d) Cyclic pressure response to 49 kPa applied pressure for 1000 consecutive cycles.

Conclusion

- Glycerol soaking procedure can effectively prevent water loss, hence improving the structural stability of CG_PEDOT:PSS system.
- CG/PEDOT:PSS organohydrogels are capable of serving as competitive strain and pressure sensors due to their exceptional stretchability and electrical properties.



Unravel the sensing mechanism the **organohydrogels system** by using small-angle X-ray scattering (SAXS).





